

## Research Article

# Changes in Cardiac Autonomic Regulation after Acute Lung Exposure to Carbon Nanotubes: Implications for Occupational Exposure

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Carbon nanotubes (CNTs) are among the most relevant engineered nanomaterials (ENMs). Given the expected rise of exposure to ENMs, there is concern that they may adversely affect health of exposed people. Aim of the study was to test the hypothesis that single wall carbon nanotubes (SWCNTs) pulmonary exposure acutely affect the autonomic cardiovascular regulation in conscious rats. We studied Wistar-Kyoto rats in which a telemetry transmitter for continuous arterial pressure (AP) and heart rate (HR) recordings was surgically implanted. SWCNTs dispersed in phosphate buffer saline (PBS) or PBS alone were randomly administered intratracheally. Immediately before, and 24 hours after each instillation a 30 min AP recording was performed. The sequence analysis was performed to evaluate the baroreflex function. In the control group, PBS instillation did not induce any significant changes. At variance the SWCNT exposure induced a significant reduction of baroreflex system (BRS) ( $3.5 \pm 0.6$  versus  $2.6 \pm 0.40$  msec/mmHg) without significant changes in the occurrence of baroreflex sequences ( $7.5 \pm 0.47\%$  versus  $7.4 \pm 0.38\%$ ). Our results show that SWCNT pulmonary exposure might affect the cardiovascular autonomic regulation thus contributing to cardiac and arrhythmic events.

## 1. Introduction

There is strong evidence that episodic high levels of airborne particulate matter (PM) are associated with stroke, heart attacks, heart arrhythmias, and sudden death [1]; these events may be precipitated, at least in part, by alterations in

the autonomic input to the heart [2–5], which can be displayed by a partial or total loss in spontaneous heart rate variability (HRV). Indeed, decreased HRV is highly predictive for increased risk of arrhythmias and sudden cardiac death [6], especially in subjects with ischemic heart disease [7].

There are also reports showing that higher levels of ambient air pollutants increase the risk of emergency department (ED) visits for cardiac arrhythmia [8]. Moreover it has been suggested that alterations in the autonomic tone eventually due to increased environment air pollution might contribute to the instability of a vascular plaque or initiate cardiac arrhythmias thus representing a plausible explanation for the occurrence of acute cardiovascular events, such as increased myocardial infarctions [9].

However, previous studies on PM have shown that ultrafine (UF) particles are more cytotoxic, inflammatory, and fibrogenic on an equivalent mass basis than fine-sized particles of the same composition. It is therefore not surprising that a recent large European study showed that the ultrafine (UF) component of PM is the major factor contributing to the alterations of cardiovascular autonomic control [10]. The responsible underlying mechanisms remain unclear but may involve activation of pulmonary neural reflex arcs, direct effects of pollutants on cerebral areas responsible for autonomic control or on cardiac ion channels, or may follow the heightened systemic inflammatory state.

Synthetic nanomaterials, developed in recent years to engineer new structures, materials, and devices, generally occur in size ranges similar to UF particles. An important class of synthetic nanomaterials is represented by carbon nanotubes. These cylindrical carbon molecules have novel properties, making them potentially useful in many applications in nanotechnology, electronics, optics, and other fields of materials science, as well as potential uses in architectural fields. Therefore, their wide utilization raises concern about possible adverse effects on cardiovascular system. Indeed, some preliminary animal data suggest that carbon nanotubes may promote atherosclerosis [11].

No definitive data are currently available on their possible effects on the cardiovascular autonomic control.

The introduction of techniques able to monitor arterial pressure and heart rate in conscious, freely moving animals allows to evaluate possible modifications of autonomic cardiovascular regulation over time in response to various experimental conditions [12]. In particular, the possibility to monitor the baroreflex control of sinus node by studying the baroreflex sensitivity (BRS), in a noninvasive and nonobtrusive way [13], is really intriguing due to its prognostic value in cardiovascular diseases [14, 15].

Therefore aim of the present study was to test the hypothesis that single wall carbon nanotubes (SWCNTs) pulmonary exposure in a physiological model of conscious rat acutely affect the autonomic cardiovascular regulation and in particular the arterial baroreflex function which has been widely considered as a predictive index of cardiac mortality in patients affected by ischemic heart disease and myocardial infarction [14, 15].

## 2. Material and Methods

**2.1. SWCNT Preparation.** SWCNTs (CarboLex, Aldrich, Steinheim, Germany) produced by the arc-discharge process, employing CO in a continuous-flow gas phase as the carbon

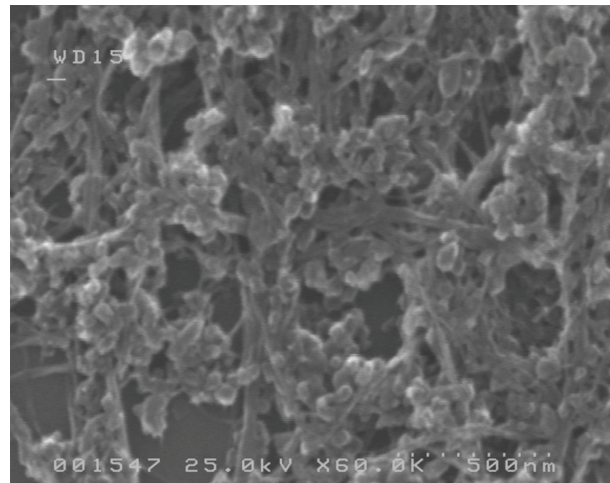


FIGURE 1: Scanning electron microscopy imaging of SWCNTs administered to rats. A high degree of agglomeration is evidenced.

feedstock and  $\text{Fe}(\text{CO})_5$  as the iron-containing catalyst precursor and purified by the  $\text{HNO}_3$  acid treatment at room temperature, were used in this study. For the SWCNTs morphological and structural characterization, Raman spectroscopy and scanning electron microscopy (SEM) were routinely used to characterize the as-received nanotube samples and the samples submitted to the purification processing steps. The Raman spectroscopy revealed a typical spectrum associated with the radial breathing mode (RBM) of carbon atoms, representing the fingerprint of single-walled carbon nanotubes. The analysis of the Raman signals in the tangential modes of the graphite lattice allowed information about the phase purity of the purified carbon nanotubes. This last showed a Raman spectrum unaffected by the acidic treatments.

**2.2. Physicochemical Characterization.** Purified suspended SWCNTs were used in the study at the final concentration of 1 mg/mL. The range of diameter and length and surface area of SWCNTs were 1.2–1.6 nm, 2–5  $\mu\text{m}$ , and 300  $\text{m}^2/\text{g}$ , respectively. Surface area was determined by Brunauer, Emmett, and Teller analysis (BET method). Carbon nanotubes were suspended in phosphate-buffered saline (0,1 M PBS, pH 7.4); immediately before the pulmonary exposure, they were sonicated for 10 minutes with a Branson Sonifier B-12 (Cell Disruptor, Sonic Power Company Danbury Connecticut at 100 W) in order to obtain a better dispersion of the nanomaterial. The choice to disperse SWCNTs in PBS was taken in order to reproduce the same experimental conditions of a previous relevant study showing a proatherosclerotic effect after intratracheal instillation of SWCNTs [11]; the 10 min sonication procedure was chosen because in preliminary experiments we found that after 10 min sonication, the dispersion remained stable up to 1 min. However, as shown in Figure 1, a high degree of agglomeration was detectable at scanning electron microscopy. During all the instillation experiments, the purified SWCNT dispersion was subjected

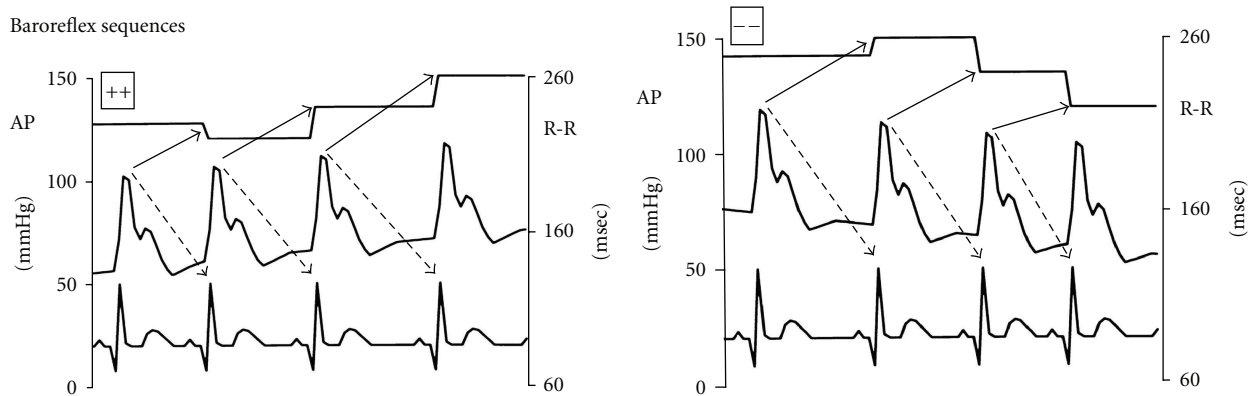


FIGURE 2: Examples of the arterial pressure, ECG signals and of the corresponding pulse intervals. The signals refer to sequences during which SAP and PI of the fifth heart beat (i.e., lag 5, used for the high heart rate of rats, see Section 2 for details) changed in the same direction, either increasing, hypertension/bradycardia, or decreasing, hypotension/tachycardia (baroreflex sequences).

to the ultrasonic bath (LBS2, 135 W) for 10 minutes, and instilled intratracheally within 1 minute after sonication, to ensure stability of the homogeneous SWCNT dispersion. The amount of SWCNTs given during each session was  $1 \mu\text{g}/\text{gr}$  body weight. This concentration is in the lower range of the dosage given in previous experimental studies aimed at assessing lung and cardiovascular toxicology of SWCNTs [11, 16, 17].

**2.2.1. General Procedures.** The study was performed on 16 adult Wistar-Kyoto (WKY) rats of both sexes (350 g body wt) and the experimental procedures were carried out according to the Association for Assessment and Accreditation of Laboratory Care International and approved by the animal care facility (Stazione per la Tecnologia Animale) of the University “Tor Vergata” and by the Italian Health Minister. Rats were used and housed individually in the animal care facility, allowed to normal rat chow and drinking water ad libitum, and kept on a 12 h light-12 h dark cycle.

**2.2.2. Surgical Procedures.** As previously described [13], after having induced the anesthesia by Ketamine (Ketavet 50 mg/kg i.p.) and Medetomidine (Domitor 0.3 mg/kg i.p.) a telemetry transmitter (TA11PA-C40, Data Sciences, St. Paul, MN, USA) was implanted for recordings of AP signals according to manufacturer specifications. The tip of the arterial catheter was inserted into the abdominal aorta previously exposed by a midline incision via a hole made by a 21-gauge needle below the bifurcation of the renal arteries just proximal to the iliac bifurcation and secured in place with tissue glue (Vetbond, 3M). The transmitter body was attached to the abdominal wall along the incision line with sutures as the incision was closed. After surgery, the rats were given antibiotics (ceftriaxone) and housed individually in cages for 5–7 days of recovery before any experimental protocol began.

**2.2.3. Measurement of Arterial Pressure Using Radiotelemetry.** As previously reported [13] the system used to record arterial pressure consists of three basic elements: (1) a transmitter for

monitoring BP (TA11PAC40); (2) a receiver (RPC-1); (3) an adapter (R11CPA) with an ambient pressure monitor (APR-1) that produces analog output signals of pulsatile AP. The telemetered AP signal was digitized using an analog I/O PC card (National Instrument 6024E, Austin, TX, USA) at a rate of 2000 Hz, displayed on the computer screen and processed by an algorithm based on feature extraction to detect and measure the characteristics of AP cycles developed in our laboratory based on a Lab view platform software. Pulse interval (PI) was measured from the pressure pulses and used to calculate heart rate (HR).

**2.2.4. Experimental Protocol.** Rats were randomly divided into two groups: control rats ( $n = 7$ ) and SWCNT instilled rats ( $n = 9$ ). SWCNTs or PBS were given to SWCNT instilled and control group, respectively. Briefly, after having induced the anesthesia as previously described, the trachea was intubated with a polyethylene cannula of the same diameter and the instillation was performed. Rats in both groups underwent 30 min duration AP recordings performed in baseline conditions and 24 hours after the instillation.

**2.3. Baroreflex Analysis by “Sequence Technique”.** The sequence analysis was performed as previously reported [13, 18]. Briefly, the beat-by-beat time series of systolic arterial pressure (SAP) and PI were analyzed by a computer to identify spontaneously occurring sequences of three or more consecutive beats in which SAP and PI of the fifth heart beat (i.e., lag 5, used for the high heart rate of rats) [19] changed in the same direction, for example, SAP increasing and PI increasing (i.e., hypertension and bradycardia) or SAP decreasing and PI decreasing (i.e., hypotension and tachycardia). These sequences were identified as “baroreflex” sequences (Figure 2). A linear regression was applied to each individual sequence, similarly to the Oxford technique employing bolus injections of vasoactive drugs. Only those sequences in which  $r^2$  was  $>0.85$  were accepted and the number of baroreflex sequences was calculated.

The mean individual slope of the baroreflex sequences, obtained by averaging all slopes computed within a given experimental period, was calculated and taken as a measure of the baroreflex sensitivity (BRS) for that period [18].

The engagement time was also calculated as the fractional occurrence of the sequences independently on recording time and/or HR as previously reported [13]. Briefly, this index has been obtained by dividing the sum of the R-R organized in sequences, according to the criteria reported above, by the total recording duration and multiplying it by 100.

**2.4. Power Spectral Analysis.** The heart rate variability (HRV) was assessed in the frequency domain by computing the power spectral density (PSD) in selected frequency bands.

As expected, dealing with conscious and freely moving animals, the 30 min RR recordings showed periods of non-stationarities both in mean and standard deviations. To comply with the requirements of the analysis we first processed all the recordings to extract stationary epochs (in weak sense). To this aim a mixed, automatic and visual, procedure was applied. First, mean, standard deviation (SD) and slope of the linear trend were computed over nonoverlapping intervals of 1 min spanning the whole recording. The selection of stationary intervals was then performed by visual inspection of the time course of mean, SD, and slope values. Stationary intervals of different lengths were detected inside the recordings: for uniformity of analysis a 5 min stationary interval was selected for each animal.

Spectral estimation was performed using Welch's averaged modified periodogram method with a Hamming window and a minimum of 50% epochs overlap. The variable overlap comes from the choice of having, for each animal, at least a preset minimum number of epochs to average. PSD was assessed in the frequency range of 0.2–6 Hz involving very low frequency (VLF: from 0 to 0.2 Hz), low frequency (LF: from 0.2 to 0.6 Hz), and high frequency (HF: from 0.6 to 3.0 Hz) spectral bands [20]. According to the literature, the PSD values VLFn, LFn, and HFn, expressed in normalized units, are obtained as the ratio between the VLF, LF, and HF powers and the cumulative power LF + HF, respectively, [21, 22].

In addition, the ratio of low-frequency (LF) to high-frequency modulation (HF) of the RR intervals which is considered to be an indirect marker of the sympathovagal balance (LF/HF) was also assessed [7]. All the software code was written in Matlab 7.10.

**2.5. Data Analysis and Statistics.** AP data were stored and analyzed by a computerized on line system for biological data elaboration developed in our laboratory based on a Lab view platform software.

Within groups changes in the reported variables were evaluated by one-way ANOVA for repeated measures for normally distributed variables and by Kruskal-Wallis one way ANOVA on Ranks for nonnormally distributed variables. The significance of differences of baseline values between the two experimental groups was evaluated by *t*-test. All data are

TABLE 1: Comparison of cardiovascular and autonomic values in baseline (i.e., before intratracheal instillation of either PBS or SWCNTs) condition between control and SWCNT instilled rats.

|                  | Control ( $n = 7$ ) | Instilled ( $n = 9$ ) |    |
|------------------|---------------------|-----------------------|----|
| SAP (mmHg)       | $130.7 \pm 5.1$     | $127.2 \pm 5.0$       | NS |
| DAP (mmHg)       | $99.9 \pm 4.4$      | $95.8 \pm 3.2$        | NS |
| HR (b/min)       | $333.1 \pm 17.0$    | $351.6 \pm 12.0$      | NS |
| BARO%            | $8.3 \pm 0.7$       | $7.5 \pm 0.5$         | NS |
| BRS (msec/mmHg)  | $4.1 \pm 0.9$       | $3.5 \pm 0.6$         | NS |
| NBARO%           | $4.1 \pm 0.5$       | $3.9 \pm 0.2$         | NS |
| NBRS (msec/mmHg) | $4.1 \pm 0.9$       | $3.4 \pm 0.5$         | NS |

Mean values  $\pm$  SEM. SAP: systolic arterial pressure; DAP: diastolic arterial pressure; HR: heart rate; BARO%: engagement time for baroreflex sequences; BRS: baroreflex sensitivity; NBARO%: engagement time for nonbaroreflex sequences; NBRS: gain of the nonbaroreflex sequences. Statistical analysis has been performed by one-way repeated measures analysis of variance or Friedman repeated measures analysis of variance on ranks tests.

presented as means  $\pm$  SEM. A value of  $P < 0.05$  was considered statistically significant.

### 3. Results

In baseline conditions (i.e., before intratracheal instillation of either PBS or SWCNTs) cardiovascular parameters did not differ between control and SWCNT instilled rats (Table 1) and no significant cardiovascular changes were evident after 24 hours (Figure 3) in both experimental groups.

Similarly the occurrence of baroreflex sequences and BRS in baseline conditions did not show significant changes between control and SWCNT instilled rats (Table 1). Also the indexes evaluating the spectral analysis of the heart rate variability were similar in baseline condition between the two experimental groups and in particular LFn was  $0,079 \pm 0,01$  for control group and  $0,066 \pm 0,009$  for SWCNT instilled rats, HFn  $0,402 \pm 0,06$  versus  $0,261 \pm 0,05$ , VLFn  $0,519 \pm 0,07$  versus  $0,673 \pm 0,05$ , and LFn/HFn  $0,209 \pm 0,02$  versus  $0,342 \pm 0,07$ .

The power spectral analysis of the heart rate variability did not appear to be affected by the SWCNT experimental acute exposure. In fact LFn, HFn, VLFn, LFn/HFn did not show significant changes between basal condition and after 24 hour from the instillation both in the control and in the SWCNT instilled rats (Figure 4).

In the control group the PBS instillation did not induce any significant changes in the occurrence and in the sensitivity of baroreflex sequences (Figure 5). At variance the SWCNT experimental acute exposure induced a significant reduction of BRS without significant changes in the occurrence of baroreflex sequences (Figure 5). These differences are not trivial because whereas in SWCNT instilled rats the significant reduction accounts about 21% for BRS, in the control group BRS shows an increase of about 51%. Indeed the BRS percent changes from baseline versus acute exposure are significantly different between PBS and SWCNT instilled rats (Figure 6).



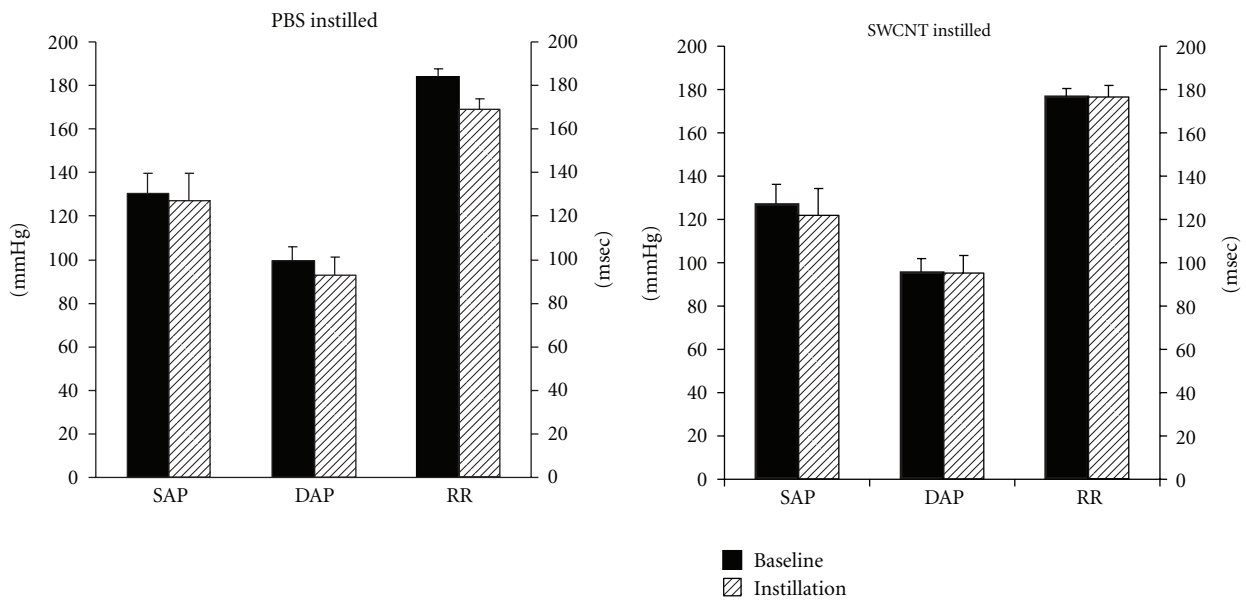


FIGURE 3: Systolic (SAP), diastolic (DAP) arterial pressure, and RR interval values before and after acute instillation of, respectively, PBS (control group) and SWCNTs (experimental group).

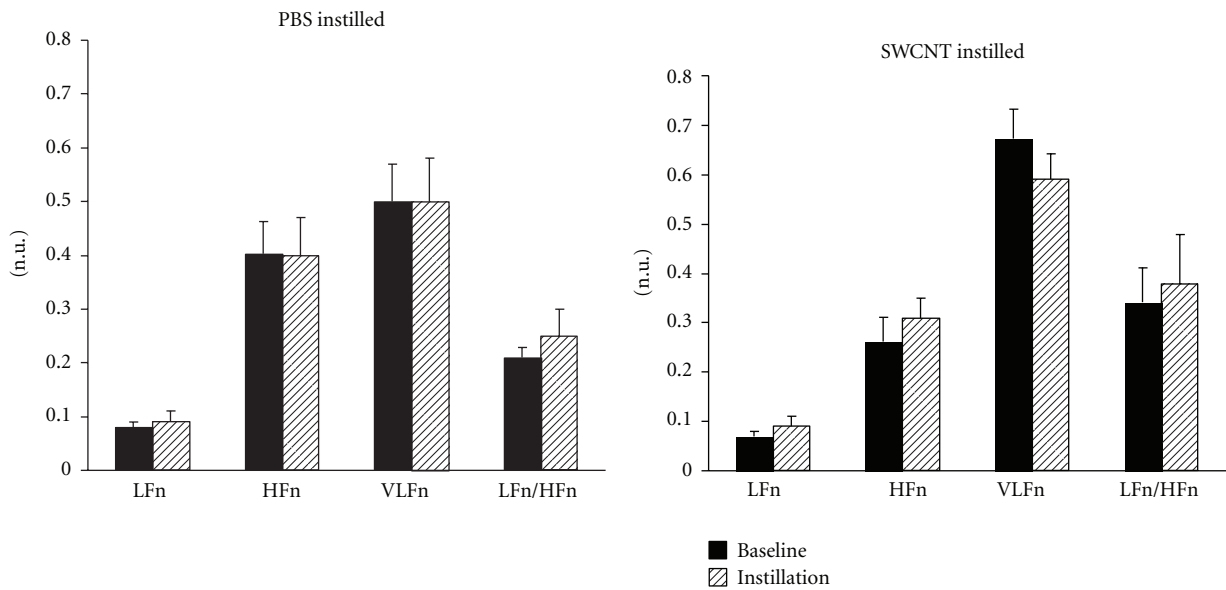


FIGURE 4: Differences in the frequency domain indexes of heart rate variability obtained by computing the power spectral density (see Section 2 for the details) in response to acute instillation of, respectively, PBS (control group) and SWCNTs (experimental group). LFn: low frequency values expressed in normalized units; HFn: high frequency values expressed in normalized units; VLFn: very low frequency values expressed in normalized units; LFn/HFn: the ratio of normalized low-frequency (LF) to high-frequency modulation (HF) of the RR intervals which is considered to be an indirect marker of the sympathovagal balance (LFn/HFn).

The mean prevailing systolic arterial pressure determining the operating point at which the baroreflex and non-baroreflex sequences were calculated did not differ significantly after the instillation both in the control and in the experimental group (127,2 mmHg in baseline condition versus 121,9 mmHg after SWCNT instillation and 130,7 mmHg in baseline condition versus 127,4 mmHg after the instillation in control group).

#### 4. Discussion

The main goal of the present investigation was to study the autonomic cardiovascular regulation in response to acute pulmonary exposure to carbon nanotubes. The distinctive aspect of the present study has been to utilize a physiological model of conscious freely moving rats in order to avoid any possible and well known interference of anesthetic drugs

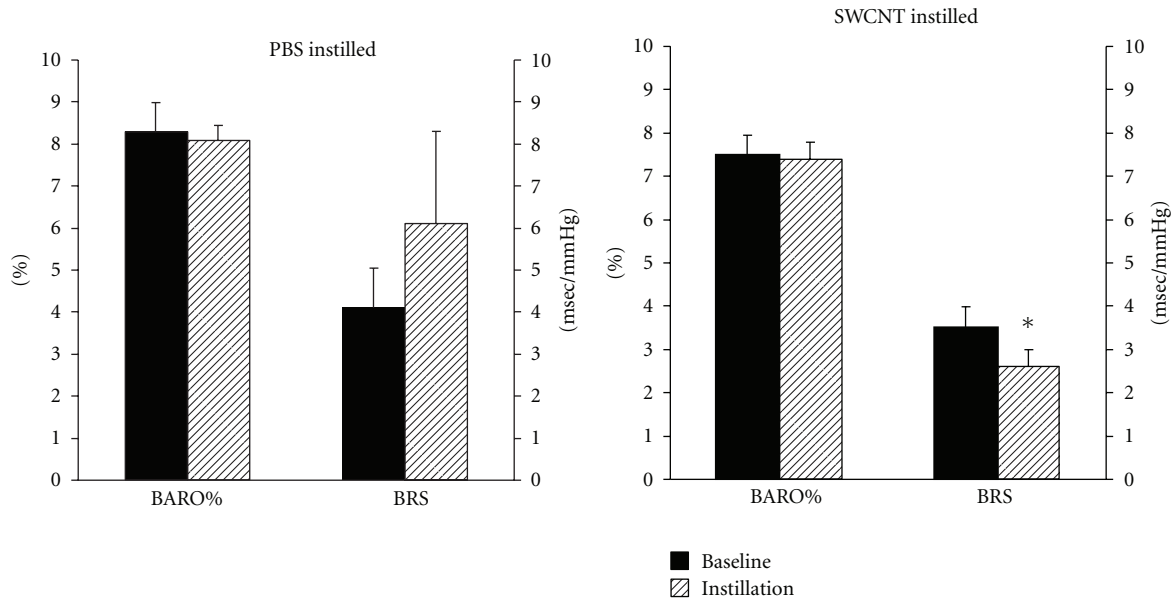


FIGURE 5: Occurrence of baroreflex sequences (BARO%), baroreflex sensitivity (BRS) before and after acute instillation of, respectively, PBS (control group) and SWCNTs (experimental group). Asterisk indicates a significant difference ( $P < 0.05$ ).

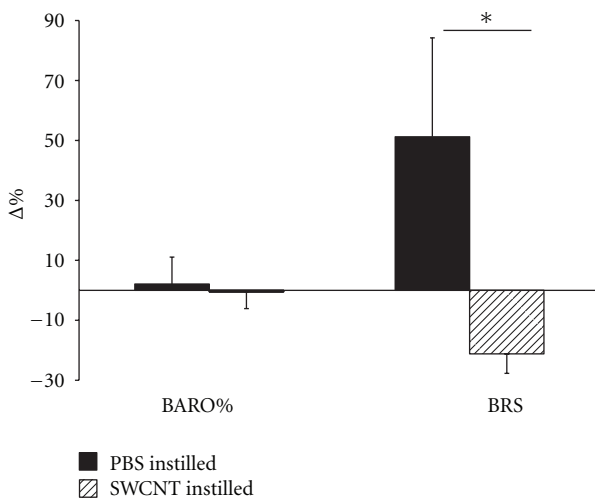


FIGURE 6: Percent changes of baroreflex sequences (BARO%), baroreflex sensitivity (BRS) after acute instillation of, respectively, PBS (control group) and SWCNTs (experimental group) from baseline values. Asterisk indicates a significant difference ( $P < 0.05$ ).

and other experimental tools routinely used in acute experimental models.

It has been largely reported that airborne particulate matter (PM) is associated with cardiovascular diseases and in particular with acute events thus increasing the ED visits [8]. Moreover UF particles seem to cause an alteration of the cardiovascular autonomic regulation [10]. Less data exist concerning the effect of synthetic nanomaterials even though their size is similar to UF particles. In particular the attractive properties of nanomaterials for medical and technological applications induces an increase in their utilizations and

therefore a growing level of possible exposure to these materials.

Concerning the cardiovascular system, previous studies have shown that carbon nanotubes have the potential effect of promoting atherosclerosis [11].

Our study shows for the first time that acute pulmonary exposure to SWCNTs causes a reduction of BRS in conscious freely moving rats.

In fact in the control group PBS instillation induced a non significant increase in BRS whereas in the experimental group SWCNT instillation produced a significant BRS reduction. Even when considered as percent change from control values, the responses to PBS and to SWCNTs resulted significantly different despite the relevant data dispersion as demonstrated by SEM (Figure 6).

In the intact circulation beat-by-beat spontaneous arterial pressure fluctuations have been shown to be linked to beat-by-beat spontaneous changes in RR interval through baroreflex mechanisms. On this basis the “sequence” technique [23] is able to extract from SAP and RR time series sequences of spontaneously occurring consecutive beats in which SAP and RR of the following beat change in the same direction, that is hypertensive/bradycardic (SAP+/RR+) and hypotensive/tachycardic sequences (SAP-/RR-). These sequences have been named “baroreflex sequences” and have been considered as expression of negative feedback mechanisms of baroreflex origin [2] (Figure 2).

The introduction of techniques able to monitor arterial pressure and heart rate in conscious freely moving animals allows to evaluate possible modifications of autonomic cardiovascular regulation over time in response to various experimental conditions [12]. In particular, the possibility to monitor the baroreflex control of sinus node by studying the baroreflex sensitivity (BRS), in a noninvasive and

nonobtrusive way [13] is really intriguing due to its prognostic value in cardiovascular diseases [15]. Indeed a pilot study from our group suggested the feasibility to evaluate the arterial baroreflex function [24] in response to SWCNT pulmonary exposure in conscious freely moving rats. Moreover, autonomic cardiovascular regulation has been investigated by means of power spectral analysis of HR and BP variability, a technique currently used to derive noninvasive indexes of the different neural components modulating the sinoatrial node and the autonomic vascular outflow [7].

The possibility to analyze the cardiovascular autonomic pattern and in particular the arterial baroreflex function is relevant because it has been widely shown that alteration in the autonomic modulation of the cardiovascular system has an important prognostic and predictive value in patients affected by cardiovascular disease. In particular several studies have indicated that a depressed BRS, an index of the reflex vagal control of the sinus node is associated with a greater risk for ventricular fibrillation during transient ischemia after myocardial infarction [25, 26]. The unfavorable effect of a depressed BRS on ventricular arrhythmias during myocardial ischemia also extends to animals without prior myocardial infarction [26]. Moreover, clinical studies have clearly demonstrated that BRS is markedly depressed during spontaneous episodes of transient myocardial ischemia [27] and in patients without a myocardial infarction who experienced out-of-hospital ventricular fibrillation [28].

Therefore the possibility that the reduced BRS in response to SWCNT acute exposure, shown in the present study, might contribute to the increased cardiovascular risk connected to high levels of airborne particulate matter, as constituted both by PM and UF matter, must be taken into account. Indeed increased levels of environmental UF particulate have been reported to be linked to increased ED access for cardiac arrhythmias [8].

It is noteworthy that the power spectral analysis has not shown significant changes in response to acute SWCNT exposure. This is an important information, because BRS and power spectral analysis, as tools to extract physiological information from the heart rate variability, reflect different, although possibly related [29], aspects of the autonomic modulation of the heart rate and are not clinically redundant [15, 30]. Although both BRS and heart rate variability effectively discriminate individuals at high and low risk for cardiac mortality [15], experimental [31], and clinical [32–34] studies have indicated that BRS is more useful in the prediction of future cardiac events in patients affected by ischemic cardiac disease. Another possible alternative explanation is that our analysis has been performed on 5-min intervals, a time in which is possible to evaluate only the short-term HRV thus losing information that could be present in the whole-time interval. Furthermore, it must be pointed out that power spectral analysis is a tool belonging to the field of the so-called linear analysis and does not take into account possible nonlinear variations occurring between the two conditions.

Overall these data might suggest that the autonomic cardiovascular regulation is affected by acute SWCNT exposure by acting on the negative feedback mechanisms of baroreflex

origin, mainly vagally mediated. These data may have relevance from an occupational perspective. In fact, given the expected widespread production of CNTs-based goods, an accidental exposure at work may be considered possible. Not surprisingly, case-reports, regarding adverse outcomes after accidental exposure to manufactured nanomaterials are starting to be reported [35–37]. Another point to be considered is that a substantial amount of workers have chronic cardiovascular disorders: these workers are highly sensitive to the adverse effects of altered cardiac autonomic regulation, and thus the effects observed in this experimental study might be seen at corresponding lower doses and might also be more severe than those reported here.

In conclusion, the results of the present study show that SWCNT pulmonary exposure might alter the physiological autonomic regulation thus contributing to cardiac and arrhythmic events as reported in response to PM and UF particles exposure.

*Limitation.* The generalization of the BRS response to SWCNT exposure to the whole population including also patients affected by cardiovascular diseases and in particular ischemic cardiac disease represents a limitation of this study. Therefore, it would be desirable to extend the present study to an animal model of experimentally induced myocardial infarction in order to test the hypothesis that the BRS depression induced by SWCNT exposure might also occur in patients affected by myocardial infarction.

However, considering that it has been clearly reported by clinical studies that both BRS and heart rate variability are reduced after a myocardial infarction [14] and that BRS is markedly depressed during spontaneous episodes of transient myocardial ischemia [27] and in patients without a myocardial infarction who experienced out-of-hospital ventricular fibrillation [28], it is conceivable that an eventual BRS reduction in response to SWCNT exposure in patients affected by ischemic cardiac disease might represent an environmental risk factor for developing life-threatening arrhythmic events.

Also the limited experimental sample reported in the present study might have biased some results. For this reason further experiments are needed to definitively confirm our findings.

## Conflict of Interests

The authors have no conflict of interests to declare.

## Acknowledgments

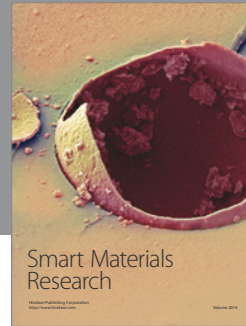
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